

# A novel approach to modeling state-related fMRI activity using change-point theory

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## INTRODUCTION

Goal: To develop and apply a hybrid hypothesis- and datadriven analysis for modeling sustained psychological states with uncertain onset time and duration; e.g., experienced emotion, learning, insight.

 Need to balance inferential power of hypothesis-driven approaches (e.g. GLM) with flexibility of data-driven methods (e.g. ICA).

Our approach: Uses ideas from statistical control theory and change point analysis

- · Population inference on whether and when a time series changes from a baseline state
  - Handles uncertain onset times and durations

Simulations: false-positive rate (FPR) control and power Application: fMRI study (n = 25) of state anxiety.

Toolbox: Matlab implementation freely available

http://www.columbia.edu/cu/psychology/tor/

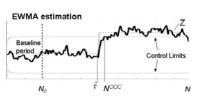


Figure 1. A schematic overview of the model of true activation (boxcar) and the EWMA statistic  $z_i$  (black line). Control limits for EWMA statistic deviations can be calculated as  $cVar(z_i)$ , where c is a critical t-value corresponding to the desired false positive-rate

### **METHODS**

Our method is a multi-subject extension of the exponentially weighted moving average (EWMA, Fig. 1) method used in change-point analysis. The analysis uses activity collected during a baseline period to estimate noise characteristics in the signal, and then make inferences on whether, when, and for how long subsequent activity deviates from the baseline level. We extend existing EWMA models for individual subjects (a single time series) so that they are applicable to fMRI data, and develop a group analysis using a hierarchical model, which we term HEWMA (Hierarchical EWMA). The HEWMA method can be used to analyze fMRI data voxel-wise throughout the brain, data from regions of interest, or temporal components extracted using ICA or similar methods.

### Detecting Change points

 No a priori assumptions about the nature of changes in the fMRI signal. Can handle activation or deactivation, short or prolonged activation duration.

· EWMA is a search for activity differences across time, correcting for multiple dependent comparisons tested

EWMA

• Given observations in time  $X = (x_1, x_2, \dots x_n)$ 

• Two-state model: baseline ("in-control") and activated ("out of control"). Assume data is distributed normally:  $N(\theta_0, \Sigma)$  for baseline and  $N(\theta_1 \Sigma)$  for activated.

θ<sub>o</sub> is estimated from pre-specified baseline period

• After baseline, process is "in control" up to some unknown time  $\tau$ , the change point (CP), when the state changes to activated (see Fig. 1). . The exponentially weighted moving-average (EWMA) statistic, , is a temporally smoothed version of the data, which is defined as:

$$z_t = \lambda x_t + (1 - \lambda) z_{t-1} \text{ for } t = 1, \dots n \quad [1]$$

where  $0 \le \lambda \le 1$  is a constant smoothing parameter chosen by the analyst (small  $\lambda$  gives more smoothing), and the starting value  $z_0$  is set equal to the baseline estimate of θ<sub>0</sub>

• To test whether the process has changed states at time t, we compute a test statistic for each time point following the baseline:

$$T_{t} = \frac{\left|z_{t} - \theta_{0}\right|}{\sqrt{Var(z_{t})}}$$

[2]

where Var(z<sub>t</sub>) is the (co-)variance of the EWMA statistic at time t.

• Theoretical results for Var(z<sub>t</sub>) for a variety of noise models is provided in Lindquist and Wager (2006).

· Under the null hypothesis T follows a t-distribution.

- · Family-wise error rate control across the time series is provided using Monte Carlo integration
  - Generate null hypothesis data with covariance given by  $Var(z_i)$ Save the maximum absolute T-value obtained across the time series
  - Compare observed T values against distribution of maxima

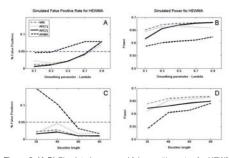


Figure 2. (A-B) Simulated power and false positive rates for HEWMA with varying smoothness parameter, and fixed baseline length of 60 • Iterative estimation of Zpop and its variance components. TRs. (C-D) Same plots with fixed lambda and varying baseline length.

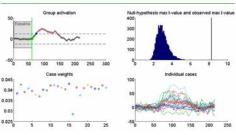


Figure 3. (A) HEWMA group activation, Z<sub>pop</sub>, and the estimated CP **Clustering into regions** (green line). (B) Results of Monte Carlo simulations for finding • A natural unit of analysis is a multi-voxel region whose voxels show corrected p-values. Black line; observed max T; distribution; null similar properties We first obtain a Change Point Map (CPM) and hypothesis max T. (C) Case weights calculated according to Eq. (3). Activation Duration Map over all significantly activated voxels (D) The time courses for the 25 subjects

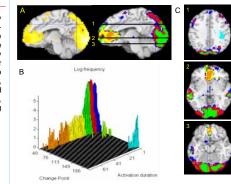


Figure 4. A) Left: Regions with significant activations in HEWMA (corrected over time and FDR-corrected over space). Right: Regions color-coded according to K-means classification (7 classes). B) Histogram of number of voxels by CP and activation duration, color coded by estimated class. C) Axial slices of regions shown in A

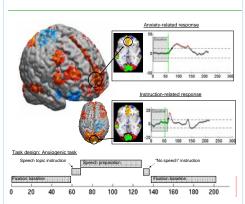


Figure 5. The brain surface is shown in lateral oblique and axial views. Significant voxels are colored according to significance. Increases are shown in red-yellow, and decreases are shown in lightdark blue. (A) Time course from a region showing sustained activity in rostral medial PFC (single representative voxel). The baseline period is indicated by the shaded gray box, and the HEWMA-statistic is shown by the thick black line (+/- one standard error across shown by the unit black interpretation of the statistical of the statistical and the statistical and the statistical statistical and the statistical s presentation of task instructions in visual cortex.

HEWMA: A hierarchical extension of EWMA

- · There is interest in fMRI in population inference
- · Approach: EWMA for each subject; mixed-effects (hierarchical) test of significance across subjects at 2nd level

Suppose the EWMA statistic at time t for subject i, which we denote  $Z_{\rm th}$  is defined as in Eq. 1. The HEWMA statistic is a weighted average of the individual EWMA statistics, with the weights inversely proportional to the total variance for each subject, i.e.

$$Z_{pop} = \left[\sum_{i=1}^{m} W^{i}\right]^{-1} \sum_{i=1}^{m} W^{i} Z^{i}$$

$$[3]$$

where  $W_i = \left(\sum_{i=1}^{n} \sum_{j=1}^{n}\right)^{-1}$ . Here  $\sum_{i=1}^{n}$  is the variance from the single subject EWMA analysis and  $\Sigma_b^*$  is the between subject variance, known up to a scaling parameter a.

• Estimate  $\alpha$  using a restricted maximum likelihood (ReML) approach

. The final step in the HEWMA framework is performing a Monte Carlo simulation to get corrected p-values, except here we use Zpop and its covariance matrix in the simulation.

Estimating Change points (CPs) If a systematic deviation from baseline is detected, we estimate the time of change and recovery time (if any).

· Zero-crossing method: use the last time point at which the process crosses  $\theta_0$  before becoming significant. Run duration: number of contiguous activated time points

MLE method: maximum likelihood estimates of τ

· Gaussian mixture model method: 2-state (control and activated); classify time points in one of the two states. Estimate duration of activated runs as above

- K-means clustering in 2-D (CP and duration) space.
  Number of classes chosen based on histogram (Fig. 4).
- Contiguous voxels of same class are "regions"

### Simulations

 Assess the FPR and power for the HEWMA method (N = 20)  $\bullet$  Vary  $\lambda$  (Sim 1: 0.1, 0.3, 0.5, 0.7 and 0.9) and duration of the baseline period (Sim 2: 20, 40, 60 or 80 time points)

• Error models in EWMA estimation: white noise (WN), AR(1), AR(2) and ARMA(1.1).

N = 20 subjects, Σ<sub>b</sub> = 0.33 \* Σ<sub>i</sub>, 5000 replications

•FPR simulation: null hypothesis data with no activation was created using actual fMRI noise time courses

• Power simulation: As above, with active period of length 50 time points was added to the noise data, Cohen's d of 0.5.

### Experimental design

24 participants were scanned in a 3T GE magnet. Participants were informed that they were to be given two minutes to prepare a seven-minute speech, and that the topic would be revealed to them during scanning. They were told that after the scanning session, they would deliver the speech to a panel of expert judges, though there was "a small chance" that they would be randomly selected not to give the speech. After the start of acquisition, participants viewed a fixation cross for 2 min (resting baseline). At the end of this period, participants viewed an instruction slide for 15 s that described the speech topic, which was to speak about "why you are a good friend." The slide instructed participants to be sure to prepare enough for the entire 7 min period. After 2 min of silent preparation, another instruction screen appeared (a 'relief' instruction, 15 s duration) that informed participants that they would not have to give the speech. additional 2 min period of resting baseline followed, which completed the functional run (Fig. 5). During a run, a series of 215 images were acquired (TR = 2s)

# RESULTS

Simulations of group data showed that false positive rates were adequately controlled for all noise models. The HEWMA analysis on the experimental data revealed task-related changes consistent with previous literature, including activations in dorsolateral and rostral medial prefrontal cortices, middle temporal gyrus, and occipital cortex (Figs. 4 and 5). Deactivations were found in ventral striatum and (rigs. 4 and 5). Deactivations were round in ventral structurn and ventral anterior insula. K-means classification of voxels by activation onset time and duration revealed distinct patterns of responses to the task (color-coded by class in Fig. 4). Time courses for two patterns of responses are shown in Fig. 5, including a medial prefrontal region showing sustained activity throughout the anxiogenic task and an occipital region showing transient responses to the instruction periods (when visual stimuli were presented).

### REFERENCES

Lindquist & Wager. "Application of change-point theory to modeling state-related activity in fMRI". In Pat Cohen (Ed), Applied Data Analytic Techniques for "Turning Points Research. In press, 2006.